Congruence between the meshes of a combined healing abutment-scan body system acquired with four different intraoral scanners and the corresponding library file: an in vitro analysis

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Highlights

1. Intraoral scanners with different scan mechanisms didn't affect the congruence between the

library file and the scan mesh of the tested scan body system.

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Original article

<u>Full Title:</u> Congruence between the meshes of a combined healing abutment-scan body system acquired with four different intraoral scanners and the corresponding library file: an in vitro analysis

Short title: Congruence of digital implant scans

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ABSTRACT

Objectives: To investigate the congruence between the meshes of a combined healing abutment-scan body (CHA-SB) system acquired with four different intraoral scanners and the corresponding library file.

Material and Methods: A CHA-SB was fixed to an implant at the right first molar position in a dentate mandibular model and digitized by using 4 different intraoral scanners (IOSs) [TRIOS 3 (T3), Omnicam (OC), Primescan (PS), and Virtuo Vivo (VV)] (n=8) and an industrial grade optical scanner (ATOS Core 80) (n=1) to generate standard tessellation language (STL) files of the test scans (CHA-SB-STLs) and the master reference model scan (MRM-STL). A reverse engineering software (Studio Geomagic X) was used to superimpose the proprietary library file of the CHASB over the generated STL files. Root mean square (RMS) values representing the deviations between the library file and the superimposed STL files were statistically analyzed by using 1-way ANOVA (α =.05). Qualitative analysis of the deviations was performed by visual inspection.

Results: Differences between the congruence of the library file and the CHA-SB scans among different IOSs were nonsignificant (F=1.619, df= 3, P = .207). The single best result was $29 \pm 28.9 \mu m$ for OC, $30.8 \pm 29.6 \mu m$ for VV, $35.6 \pm 35.5 \mu m$ for T3, and 39.5 ± 39.2

 μ m for PS, which were all above the deviation value of the scan performed by using the industrial-grade scanner (23.2 ±23.2 μ m).

Conclusion: The dimensional congruence between the library file and the standard tessellation language file of the combined healing abutment-scan body system scans was similar when intraoral scanners with different acquisition technologies were used to scan a model with an implant.

Clinical Significance

Scans of the tested intraoral scanners may result in crowns with similar positional accuracy, given the similarities in congruence of their scans with the library file.

Keywords: accuracy, healing abutment-scan body, intraoral scanner, trueness

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1. INTRODUCTION

Impression is a critical step in implant-supported prosthetic rehabilitation [1]. Due to the rapid development of computer aided design-computer aided manufacturing (CAD-CAM) and intra oral scanners (IOSs), it is possible to digitize implants in a direct digital workflow [1-3]. This method is performed by scanning intra oral scan bodies (SBs) with an IOS [4] and has improved patient comfort with the elimination of conventional impression materials and trays, eliminates the need for a stone cast, and enables a faster and more efficient communication between the clinician and the laboratory [1, 5-7].

Various types of SBs in different shapes, sizes, surfaces, and connections have been marketed over the years [1, 3]. However, the geometry of a conventional SB or coded healing abutment (HA) generally does not concur with the anatomical shape of a natural tooth [1]. It can also be difficult to accurately position a SB on an apically placed implant with the presence of thick mucosa and repeated removal and placement of an HA in these situations may jeopardize the integrity of the peri-implant soft tissues [1]. Recently introduced combined HA-scan body (CHA-SB) system overcomes these problems as it consists of an HA that contours the peri-implant soft tissue and a SB that is fitted into the screw access hole of the HA. This assembly enables the acquisition of the implant's position and the soft-tissues simultaneously [3, 10]. Coded (HAs) facilitate digital impressions by reducing the number of appointments to deliver definitive restorations and minimizing the trauma to soft tissues caused by the removal of the HA [8-10]. In addition, potential soft-tissue collapse, which may happen during the removal of a custom HA or interim prosthesis that was used to anatomically shape the peri-implant soft tissues, is eliminated [10].

IOSs depend on different data acquisition mechanisms such as confocal microscopy, optical triangulation, interferometry, active wave front sampling, stereophotogrammetry

structured light, laser, and video [2, 4, 11]. Previous studies have shown that a wide range of factors [12, 13], including IOSs, affect the accuracy of a scan [4, 6, 14-21]. However, an accurate scan is only the initial stage of the digital workflow of an implant-supported restoration. After the scan, the SB mesh is replaced with the corresponding CAD file in the library. It is preferable to design the definitive restoration using the CAD library file as it is geometrically optimal, whereas the mesh is an approximation of the scanned data to the actual geometry of the object. A definitive restoration designed by using the library file would lead to improved marginal adaptation [22, 23]. Therefore, dimensional congruence between the library file and the mesh is essential for an optimal restoration [24, 25], and has been investigated only once when different IOSs were used [22]. The SBs evaluated in that study [22] did not include an HA. A previous study has evaluated the accuracy of scans of the new CHA-SB system when 4 different IOSs were used [26], while another study compared the accuracy of CHA-SB scans with a regular scan body [3]. However, those studies [3, 26] did not focus on the dimensional congruence of this system. Considering the limited knowledge on the dimensional congruence of SB meshes with library file and the CHA-SB system in implant dentistry, an investigation combining these two factors could help clinicians to broaden their knowledge on how digital implant scans are processed in the CAD software. Therefore, the purpose of this study was to compare the dimensional congruence between the CHA-SB meshes generated from scans of 4 different IOSs with different data acquisition mechanisms and the CAD library file. The null hypothesis was that the IOS would not affect the dimensional congruence between the CHA-SB meshes generated from 4 different IOS scans and the CAD library file.

2. MATERIALS AND METHODS

2.1. Study Design

Figure 1 summarizes the overall methodology of the present study. A poly(methyl methacrylate) mandibular dentate master model with a single implant (4.0 mm×11 mm, Neoss ProActive Straight; Neoss Implant System, Harrogate, England) at right first molar position was fabricated. The implant was positioned with its inner slot facing buccally for the proper alignment of the HA as per manufacturer's recommendations. The index on the polyetheretherketone (PEEK) HA (Esthetic Healing Abutment, Neoss Implant System, Harrogate, England) was aligned with the buccal groove of the implant and HA was tightened. The SB (ScanPeg, Neoss Implant System, Harrogate, England) was then placed in the screw access hole of the HA [3, 10, 26, 27]. A vertical projection on the SB and a groove present in screw access hole of the HA facilitated this assembly, which was through friction (Figure 2). The components of the CHA-SB system were not disassembled throughout the study.

The master model was digitized by using an industrial optical scanner (ATOS Core 80 5MP; GOM GmbH, Braunschweig, Germany). The industrial scanner depends on the principle of triangulation and has a camera set-up with 6 µm sphere space error, 8 µm size error, 1 µm probing error, 3 µm probing error size, and 7 µm length measurement error [28]. Standard tessellation language (STL) file of the master reference model (MRM-STL) was generated with reverse engineering (Pro 8.1, GOM GmbH, Braunschweig, Germany) [4] and used as the reference.

Four different IOSs were used to scan the CHA-SB system: A confocal microscopy scanning technology IOS: TRIOS 3 (T3) (version 1.4.7.5, 3Shape, Copenhagen, Denmark); an optical triangulation and confocal microscopy technology IOS: Cerec Omnicam (OC) (version 4.6.1, Cerec Dentsply Sirona, Bensheim, Germany); a smart pixel sensor IOS: Cerec Primescan (PS) (version 5.0.0, Cerec-Dentsply Sirona, Bensheim, Germany), and a blue laser IOS with multiscan imaging technology: Virtuo Vivo (VV) (version 3.0, Dentalwings,

Montreal, Quebec, Canada). An experienced operator (G. Ç.) with more than 5 years of experience scanned the master model 8 times with each IOS in a humidity and temperaturecontrolled room under proper ambient light. A priori power analysis (power: 0.80, α: 0.05, and effect size: 0.6) based on the findings in a previous study [4] was performed to determine the number of scans per IOS. The operator rested for 5 minutes in between IOSs to prevent fatigue that may affect the quality of the scans [22]. The IOSs were calibrated before each scan in line with the manufacturers' recommendations. Each scan started from the ipsilateral (the quadrant with the implant) distal molar and the scan strategies were as follows: T3: The occlusal surface of the entire arch was captured first, followed by the lingual surface scans starting from the contralateral (opposing quadrant to the implant) distal molar. The scan was then completed by scanning the buccal surface starting from the ipsilateral distal molar

and terminating at the contralateral distal molar [29].

OC: The scan started with capturing the ipsilateral occlusal surfaces with a 45° tilt of the scanner palatally and terminated at the contralateral lateral incisor. After tilting the scanner by another 45° palatally, the lingual surfaces were scanned. The scanner was then tilted by 90° at the ipsilateral distal molar and occlusal surfaces were scanned moving mesially to the ipsilateral lateral incisor. The buccal surface scans started after a 45° buccal tilt at the contralateral lateral incisor and captured the whole quadrant terminating at the ipsilateral distal molar. Finally, the scanner was tilted by another 45° buccally scanning the buccal surfaces again until the contralateral lateral incisor. The opposite quadrant was also scanned with this sequence [30].

PS: The lingual surfaces of the arch were captured first, followed by the occlusal surface scans starting from the contralateral distal molar. The scan was then completed by buccal surface scans starting from the ipsilateral distal molar and terminating at the contralateral distal molar [31].

VV: Because the manufacturer of this IOS does not recommend a scan path, a scan pattern similar to T3 was used.

Each scan was inspected for imperfections, particularly on SB surfaces. A scan was considered complete when no major imperfections were detected [7]. IOS scans (test scans) were converted to STL files to generate CHA-SB meshes (CHA-SB-STL). In total, 33 STL files (32 CHA-SB-STLs and 1 MRM-STL) were collected. CHA-SB system's proprietary library CAD file, provided by the manufacturer, was used as the reference STL (nominal, CAD-LIB-STL) to simulate the generation of an implant CAD model.

2.2. Deviation Analysis

A reverse engineering software (Studio Geomagics v.2018.1.1, Morrisville, NC, USA) was used to measure the dimensional congruence between the CHA-SB-STLs and the CAD-LIB-STL by using the best-fit algorithm. Root mean square (RMS) was utilized to indicate the magnitude of deviations from zero between the 2 datasets (CHA-SB-STLs and the CAD-LIB-STL) [32]. A high RMS value indicated a low-degree of 3D matching in superimposed files of the CHA-SB system, which translated to low trueness [33].

All CHA-SB-STLs and the CAD-LIB-STLs were imported into the software. CAD-LIB-STL was used as the reference data. For the initial alignment, "Transform Alignment Function" of the software with N points method was used. Three different points (one point on the buccal vertical outdent on the SB and HA connection area, one point on the buccal of the triangle located on top of the SB, and one point on the distal of the triangle located on top of the SB, and one point on the distal of the triangle located on top of the SB, and one point on the distal of the triangle located on top of the SB. Then the "Best-STLs and the CAD-LIB-STL for the superimposition (Figure 3). Then the "Best-Fit Alignment" function of the software was used for further alignment and to minimize errors.

For the quantitative (mean \pm standard deviation (SD)) and qualitative (inward and outward, and minimal deviations) evaluation of the deviations between the CHA-SB-STLs

and the CAD-LIB-STLs, color-difference maps were created by using "3D Comparison Function" of the software. The color-difference maps allowed the evaluation of the distances between specific points, globally and in x, y, and z planes. The maximum/minimum deviation values were arranged to be +50/-50 μ m, the tolerance range being +10/-10 μ m (green) [34]. One experienced operator (V.R.) with 5 years of experience on digital dental technologies and 3D analysis software performed the evaluations.

2.3. Statistical Analysis

For the quantitative evaluation, the software automatically calculated the RMS in color difference maps, without the need for an additional formula. Minimum, maximum, average deviations, RMS, standard deviation (μ m), and total deviation percentage (%) values were recorded for each test scan. The same procedure was done for the MRM-STL. The data were analyzed by using 1-way analysis of variance (ANOVA) ($\alpha = 0.05$).

Qualitative evaluation was performed to understand the direction of the deviation (inward or outward) and to determine if there was minimal deviation. Screenshots were made from different angles after the best-fit alignment and color-difference map generation to visually evaluate the parts of the CHA-SB system individually and as a whole. Similar to the quantitative evaluation, CAD-LIB-STL was accepted as the reference and the same experienced operator (V.R.) executed the qualitative evaluation. The deviations were recorded for buccal, lingual, and occlusal surfaces according to the chromatic existence of red/yellow, green, or light/dark blue in color difference maps. The data of the occlusal surface were included in the analysis of the SB. Different shades of blue indicated Inward deviations (defects) and yellow, orange, and red indicated the outward deviations (excesses) [22]. Green indicated no deviation. The results were expressed as a qualitative variable.

3. RESULTS

One-way ANOVA revealed that there were no significant differences among the dimensional congruence of the CHA-SB system scans performed with different IOSs (F=1.619, df= 3, P= .207). Table 1 summarizes the descriptive statistics of the scans performed by using the tested IOSs, while the results of the pairwise comparisons are shown in Table 2.

Figure 4 illustrates the color maps generated to analyze the congruence between the CHA-SB mesh and the library CAD file for each IOS. The best single result (lowest deviation value among the scans performed) was $35.6 \pm 35.5 \mu m$ for T3, $29 \pm 28.9 \mu m$ for OC, $39.5 \pm 39.2 \mu m$ for PS, and $30.8 \pm 29.6 \mu m$ for VV. The reference scan superimposition over the library CAD file resulted in $23.2 \pm 23.2 \mu m$ of deviation, which was below the best single results from all IOSs tested.

Table 3 summarizes the qualitative evaluation of the deviations of the CHA-SB system scans made by visual inspection. The scans performed by using T3 mainly resulted in deviations that were within the tolerance range. However, inward deviations were observed on the lingual surfaces of the complete CHA-SB system and the SB. When scanned with OC, CHA-SB system showed both inward deviations or deviations within the tolerance range. For the HA, deviations were within the tolerance for both lingual and buccal surfaces, and inward deviations were observed on the buccal surface. For the SB, an inward deviation was predominant for each surface (buccal, lingual, and occlusal), and deviations within the tolerance range were also observed on the complete CHA-SB system, the HA, and the SB were mainly inward or deviations within the tolerance range. For the occlusal surface of the SB, deviations were predominantly within the tolerance range. When VV was utilized, scans of the complete CHA-SB system, HA, and SB mostly showed outward deviations or deviations within the tolerance range for buccal and lingual surfaces. For the occlusal surface of the SB, deviations were mainly within the tolerance range.

4. DISCUSSION

The scans of the CHA-SB system performed by using different IOSs resulted in similar deviations when superimposed over the library CAD file. Therefore, the null hypothesis was accepted.

A recent study investigated the dimensional congruence between the scans of an edentulous maxilla rehabilitated with 6 implants (#16, #14, #11, #21, #24, and #26) and library file [22]. The authors [22] reported significant differences among 5 IOSs (Primescan, CS3700, MEDIT i-500, ITERO ELEMENTS 5D, and Emerald S) and 1 desktop scanner (Freedom UHD) as well as different implant positions. Among the IOSs tested, PS resulted in the highest congruence $(25.5 \pm 5 \,\mu\text{m})$ with the library CAD file, which was similar to the deviation value of the desktop scanner (25.5 \pm 2.9 μ m) and CS3700 (27 \pm 4.3 μ m). Moreover, PS showed the single best result (lowest) (17 \pm 19 μ m) when compared with the other scanners quantitatively. The implant positions were also found to be effective on the dimensional congruence of the scans. The mean deviation values in scans performed by using PS ranged from 22.2 to 31 µm, SBs located at the right first premolar, left first premolar, and left first molar showing significantly higher trueness than the other SBs. The contrasting results between the present study and Mangano et al's [22] study might be related to several factors, one of which is the anatomy of the SB [1]. The CHA-SB system is more complex than a conventional SB as it consists of 2 individual parts that are assembled through friction fit and these 2 pieces are geometrically different [3, 10, 26]. The SBs used in Mangano et al's [22] study were 1-piece, which had a more uniform geometry than that of the CHA-SB system. In addition, the authors [22] stated that the flat surfaces of nearly all SBs showed the lowest deviation results. The absence of a flat surface on the CHA-SB system might have led to the higher deviation values observed in the present study. Other factors, which may have

contributed to the higher deviation values in the present study are operator difference [21], scan pattern [24, 35-38], ambient light [39], and the differences in IOSs tested [4, 6, 15-19] other than PS. Nonetheless, considering that different IOSs resulted in similar deviations, it can be speculated that definitive restorations manufactured by using these scans would also have similar positional trueness. However, this hypothesis needs further support with studies evaluating the fit and the contours (interproximal and occlusal contacts) of definitive crowns fabricated when the CHA-SB system scans are used.

Effect of IOSs on the scan accuracy of CHA-SB system was investigated in a previous study, in which IOSs tested in the present study were evaluated [26]. It was concluded that the IOSs did not affect the distance deviations of the scans, which is in line with the present study. These results might be attributed to the anatomy of the master model as it contained only one implant and no edentulous spaces. Previous studies have shown that increasing the number of implants and edentulous spaces [18, 40] led to higher deviations. Thus, different clinical situations might result in differences among different IOSs. Furthermore, the mean distance deviations reported (127 µm for T3, 124.6 µm for OC, 126.6 µm for PS, and 105.3 for VV) [26] were above the findings of the present study. However, careful interpretation of these results is necessary, since the deviation data in Çakmak et al's [26] study was based on a comparison between the scans of an industrial-grade scanner and the IOSs. The congruence between the master model mesh generated from the scan of an industrial-grade scanner and library CAD file was also evaluated in the aforementioned study to verify the fit between the HA and the SB [26]. Even though the deviation values in the present study are higher than the reported master model distance deviation (4.4 µm), a direct comparison would be misleading due to the differences in analysis and software used [41-43]. Çakmak et al [26] generated two circular planes (one at the top of the SB and one 3 mm below) that are parallel to each other in both master CHA-SB mesh and library file and calculated the linear deviations of the center

points of the circles below in x, y, and z axes. Additionally, the 3D analysis software used in Çakmak et al's [26] study (GOM Inspect) had prealignment feature for the initial alignment of the data, which was then followed by the best-fit alignment.

In another study, which compared the accuracy of scans of an anterior implant digitized either by the CHA-SB system or a conventional SB (direct and indirect workflow), similar deviation results were reported [3]. However, taking into account that CHA-SB system is a new approach in digital implant dentistry, future studies investigating different factors that might affect the scan accuracy are needed to broaden the knowledge on this system. Moreover, previous studies have shown that the accuracy of an implant scan might be affected by the manufacturing tolerances of the SBs [25, 44] as various materials are used for the fabrication of SBs [1]. Schmidt et al [25] compared the manufacturing tolerances of 3 SBs by using x-ray computed tomography and concluded that the scan accuracy might be affected by manufacturing tolerances. These findings were corroborated in a previous study [44], where different 1-piece SBs were investigated. The highest tolerances and deviations were found in vertical direction with implants that had conical connections. Unlike conventional SBs, CHA-SB has 2 pieces, which are composed of different materials. Therefore, the manufacturing tolerances of the CHA-SB system may affect the scan accuracy more significantly, which should be investigated in future studies.

This in vitro study was performed under standardized conditions. Therefore, factors like gag reflex, presence of blood or saliva, space limitation, and patient movement, which may affect the scan accuracy in clinical practice were excluded [2, 6, 7, 18]. The present study focused on the influence of IOSs on the scan accuracy of the CHA-SB system. Given the fact that the scan accuracy is affected by various factors such as the type of the IOS, the experience of the operator, the scan strategy, and the ambient light [13, 18, 21, 24, 35-39] and the present study being the first on the dimensional congruence of the CHA-SB system scans,

future studies should elaborate the findings of the present study by investigating the angular deviations of the CHA-SB system scans as well as the precision of these scans when performed by different operators.

5. CONCLUSIONS

Considering the limitations of the present study, the results suggest that the congruence between the CHA-SB scans and CAD library file was similar when tested IOSs were used. However, future studies are necessary to corroborate and to elaborate these preliminary findings, as the effect of the level of congruence between the CHA-SB scans and CAD library file on the fabricated restorations are unknown.

Author Statement

The authors of the manuscript contributed in the following ways to the submitted manuscript:

Mustafa Borga Donmez: Design, Data collection, Drafting article

Vinicius Rizzo Marques: Data collection, Data interpretation

Gülce Çakmak: Design, Data collection, Drafting article, Critical revision of article

Hakan Yilmaz: Data analysis, Data interpretation, Statistical analysis.

Martin Schimmel: Design, Critical revision of article

Burak Yilmaz: Data interpretation, Critical revision of the article, Approval of the submitted and final versions

Declaration of interests

 \boxtimes The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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All other authors have no conflicts of interest to declare. The authors do not have any financial interest in the companies whose materials are included in this article.

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TABLES

Table 1. Descriptive statistics of the CHA-SB scans performed with each IOS

IOS	Mean ±standard deviation (µm)	Min-Max deviation (µm)	95 % CI (μm)
Т3	37.8 ±2.4	35.6-41.6	35.8-39.8
OC	42.1 ±13.8	29-68.7	30.6-53.7
PS	40.4 ±0.6	39.5-42.9	39.9-40.9
VV	34.7 ±3.2	30.8-55.5	32-41.4
S	JIN OL		

IOS	Т3	OC	PS	VV
T3	-	.627	.885	.827
OC	.627	-	.963	.19
PS	.885	.963		.404
VV	.827	.19	.404	-
<i>P</i> <.05 indicate significan	t differences among groups	Rec		

Table 2. P values of the pairwise comparisons

Table 3. Distribution of the deviations on each surface of the combined healing abutment-

scan body system

		Deviation	Lingual	Buccal	Occlusal
		Inward	++	+	
	CHA-SB	Outward	+	+	
		No	+	++	
Т2		Inward	+	+	
15	HA	Outward	+	+	
		No	++	++	
		Inward	++	+	+
	SB	Outward	+	+	+
		No	++	++	++
			Lingual	Buccal	Occlusal
		Inward	++	++	
	CHA-SB	Outward	+	+	
		No	++	++	
00		Inward	+	++	
UC	HA	Outward	+	+	
		No	++	++	
		Inward	++	++	++
	SB	Outward	+	+	+
		No	+	+	++
			Lingual	Buccal	Occlusal
		Inward	++	++	
	CHA-SB	Outward	+	+	
		No	+++	++	
DC		Inward	++	++	
PS	ĤA	Outward	+	+	
		No	++	++	
		Inward	++	++	+
	SB	Outward	++	+	++
		No	++	++	+++
			Lingual	Buccal	Occlusal
		Inward	+	+	
	CHA-SB	Outward	++	+	
		No	+++	+++	
X7X7		Inward	+	+	
V V	HA	Outward	++	++	
		No	+++	+++	
		110			
		Inward	+	+	+
	SB	Inward Outward	+ ++	+ ++	+ +

* +: Less; ++: Normal; +++: More

FIGURES

Fabrication of the master model with a single implant and combined healing abutment-scan body system located at the right first mandibular molar site
Master model scan with an industrial-grade scanner (ATOS Core 80 5MP) and MRM-STL was generated (n=1)
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Test scans by using 4 different intra oral scanners (T3, OC, PS, and VV) and test-scan STLs were generated (n=8)
Superimposition of the MRM-STL and test-scan STLs (33 STLs in total) over the proprietary CAD file of the combined healing abutment-scan body system by using a reverse engineering software (Studio Geomagics v.2018.1.1)
Quantitative (RMS) and qualitative (Visual inspection of the superimposed STLs) deviation analyzes

Figure 1. Schematic representation of the study design



Figure 2. Disassembled combined healing abutment-scan body system

Figure 3. Points determined for the alignment procedure (Red: Point on the buccal vertical outdent; Green: Point on the buccal of the triangle located on top of the scan body; Blue:



Point on the distal of the triangle located on top of the scan body)

OUTROL



Figure 4. Quantitative evaluation of the CHA-SB system with colorimetric map (A: T3; B:

OC; C: PS; D: VV; E;

Reference scan; 1: Buccal; 2:

Lingual; 3: Occlusal)