## Review

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# Sonography in surveillance for HCC in NAFLD patients 

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#### Abstract

Over the last decade, we have been facing a new aetiology responsible for the development of HCC - the nonalcoholic fatty liver disease (NAFLD). The prevalence of HCC development in this group is higher than that observed in the general population and in non-cirrhotic subjects with other causes of liver disease. Conventional ultrasound (US) is the first-line tool for HCC surveillance, but, in this population, it has a decreased diagnostic accuracy due to several particular features, including obesity and steatosis. Contrast-enhanced ultrasound (CEUS) appeared as a new branch of US due to its ability to depict the vascular architecture of all types of focal lesions (FLs). Nevertheless, CEUS has several limitations besides those inherited from US, which renders this method unreliable as the first-line HCC diagnostic tool and for HCC staging. Artificial intelligence eliminates operator limitations, which has led to an increased sensitivity and specificity of US. However, this approach is still in its early stages and more data are needed. Consequently, the purpose of the current study is to highlight the strengths and limits of US, along with its alternatives to HCC screening in NAFLD population.


Keywords: Non-alcoholic fatty liver disease, hepatocellular carcinoma, conventional ultrasound, contrast-enhanced ultrasound, artificial intelligence

## INTRODUCTION

Due to the associated co-morbidities (i.e., obesity, metabolic syndrome and type 2 diabetes mellitus) and

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complications, non-alcoholic fatty liver disease (NAFLD) has become one of the leading causes of morbidity and mortality globally, affecting approximately $25 \%$ of the world's population ${ }^{[1,2]}$. NAFLD is the most common aetiology of chronic liver disease as a major cause of cirrhosis and non-viral HCC. It is expected to become the leading aetiology for liver transplantation this decade ${ }^{[1,3]}$.

Cohort studies from Italy and the United States reported that the majority of NAFLD-related HCC patients are not diagnosed through regular surveillance, resulting in a more advanced HCC stage at diagnosis ${ }^{[4,5]}$. Furthermore, several authors reported that, despite a preserved liver function, these patients are generally older with more co-morbidities, which are factors that limit the use of curative treatment leading to a worse prognosis ${ }^{[5-7]}$. Although NAFLD has a relatively low risk of HCC development, the high prevalence of NAFLD in the population and the impact on health costs underline the importance of this aetiology. Developing a risk stratification model is essential in selecting the appropriate management for each patient. Published data indicate that male patients with NAFLD are more susceptible to developing HCC than women with NAFLD at fertile age, whereas ageing and menopause are associated with an increased risk in women with NAFLD ${ }^{[8]}$. A better understanding of carcinogenesis related to NAFLD would provide important information concerning the selection of the subset of patients with a higher risk for HCC development. Different metabolic co-morbidities, such as obesity and diabetes, are being incriminated, along with the pro-inflammatory status, Hispanic ethnicity and genetic predisposition [i.e., genetic polymorphisms in patatin-like phospholipase domain-containing protein 3 (PNPLA3), transmembrane 6, superfamily member 2 (TM6SF2), glucokinase regulator (GCKR), membrane bound O-acyltransferase domain-containing 7 (MBOAT7) and hydroxysteroid 17-beta dehydrogenase 13 (HSD17B13)] $]^{[9]}$. However, there are currently no validated "risk scores for HCC development" aimed at selecting NAFLD patients ${ }^{[10]}$.

At present, the European Association for the Study of the Liver (EASL) and the American Gastroenterology Association Clinical Practice (AASLD) Update recommend HCC screening for patients with cirrhosis and consider screening in advanced fibrosis (F3) ${ }^{[1-13]}$. Since HCC occurrence has also been reported in the F0-F2 NAFLD population, there are still concerns that the HCC risk occurrence is underestimated ${ }^{[14]}$. Unfortunately, ultrasound keeps a low sensitivity in diagnosing HCC during the very early stage. Furthermore, US is an inefficient tool for HCC diagnosis in the NAFLD population due to specific sound conditions. In this context, it is obvious that we need to update the diagnostic tool to identify NAFLD patients at risk and diagnose them at an early stage. In recent years, artificial intelligence (AI) has shown encouraging results. However, since it is still in its early stages, more data are requested before it can be used in the current practice.

## CONVENTIONAL ULTRASOUND AND COLOUR DOPPLER ULTRASOUND

The aim of US is to identify any area with a different echogenicity compared to the surrounding parenchyma and not to characterise it. Hepatocarcinogenesis is a multistep process that implies the changes within the tumour (i.e., fatty content, loosing of portal vessels, increasing arterial vascularity and necrosis). All these changes are reflected in the HCC appearance, leading to variable HCC features. Depending on its size, tumour echogenicity is defined as hypo ( $23 \%-54 \%$ ), hyper ( $12 \%-38 \%$ ) or mix echogenicity $(17 \%-38 \%)^{[15]}$. The high intratumoral fat content found in $36.4 \%$ of HCC within $10-15 \mathrm{~mm}$, increases the echogenicity of HCC lesions and may mimic the appearance of a hyperechogenic lesion, such as haemangioma ${ }^{[16]}$. Conversely, haemangiomas may appear hypoechoic in severe steatosis, mimicking an HCC lesion [Figure 1].

A "halo sign" is found in HCC with a fibrous capsule, but it can be found in benign tumours as well ${ }^{[15,17]}$. Thus, based only on the information provided by B mode, a differential diagnosis is not possible, and


Figure 1. Liver haemangioma in a 40-year-old woman examined in the supine position. Conventional US revealed a hypoechoic lesion in segment VII and a liver parenchyma with an increased echogenicity (A). One year later, after the patient lost 10 kg , the known hypoechoic lesion described in segment VII had a hyperechoic appearance, typical for haemangiomas. The adjacent liver parenchyma had a significantly decreased echogenicity compared with the previous examination (B). Courtesy Dr. Delgado Gabriela, Department of Visceral Surgery and Medicine, Inselspital, Bern University Hospital, University of Bern, Bern 3008, Switzerland.
additional information concerning intratumoral vascularity is necessary [Figures 2 and 3].

Colour Doppler mode offers additional information concerning the lesion's vascularity without having the ability to establish the final diagnosis. The changes in intratumoral vascularisation that occur during tumour growth result in a shift from an afferent continuous waveform signal ( $\mathrm{HCC}<2 \mathrm{~cm}$ ) to a pulsatile afferent flow with constant efferent flow and a very high pulsatility index (large HCC) ${ }^{[18,1,1]}$.

According to a meta-analysis by Singal et al., US pooled sensitivity (Se) varied from $94 \%$ for detecting HCC at any stage to $63 \%$ for early-stage $\mathrm{HCC}^{[20]}$. Tzartzeva et al. reported the same wide variation of pooled Se of US, from $84 \%$ for HCC at any stage to $47 \%$ for early HCC ${ }^{[21]}$.

Deep localisation (i.e., segment IVa, VII or VIII) and subcapsular localisation have been associated with inappropriate tumour visualisation and a high rate of misdiagnosis ${ }^{[22,23]}$. An important aspect that needs to be considered in the NAFLD population is the associated obesity, which limits image quality. Ultrasound waves are attenuated at a rate of 0.63 dB per centimetre of fat ${ }^{[24]}$. This finding also explains why patients with predominant subcutaneous fat distribution have a lower US image quality than those with predominant visceral fat. As reported by Uppot et al., the limitations in image quality start to become evident from the weight above $250 \mathrm{lbs}{ }^{[25]}$. This was confirmed by Esfeh et al. who reported a decreased sensitivity from $59 \%$ ( $95 \%$ CI: $43 \%-74 \%$ ) in non-obese patients to $19 \%$ ( $95 \%$ CI: $10 \%-28 \%$ ) in obese patients ( $P$-value $<0.001)^{[26]}$. Technical adjustments, such as the selection of the optimal sound frequency (a low sound frequency allows a higher penetration depth), changing gain and shifting the focus to a deeper region, are necessary to improve image quality ${ }^{[27]}$.

Another aspect that must be considered is the infiltrative pattern of HCC associated with an increased risk of surveillance failure compared to the nodular type ( $57.1 \%$ vs. $2.1 \% ; P<0.001)^{[28]}$. Noteworthy, advanced HCC may coexist with a macrovascular invasion. Based on the thrombus echogenicity, US cannot differentiate between malignant and benign thrombus. Even though Colour Doppler can detect the presence of vessels, indicating malignity, the method's sensitivity is lower than $20 \%{ }^{[29]}$ [Figure 4A and B]. Thus, US visualisation of macrovascular thrombosis requires further imaging with contrast agents.


Figure 2. Conventional US revealed a hypoechoic lesion in segment VII in a 71-year-old man with non-alcoholic liver cirrhosis. Ultrasound attenuation can be observed in deep segments. The lesion was a hepatocellular carcinoma.


Figure 3. Conventional US revealed an isoechoic lesion with a hypoechoic halo in a 23 -year-old woman diagnosed with non-alcoholic liver steatosis (arrow). CEUS examination followed, and, based on the contrast behaviour, the final diagnosis was focal nodular hyperplasia.


Figure 4. Thrombosis of portal vein (main, right and left branch) in a 62-year-old man recently diagnosed with NASH-related cirrhosis in $B$ mode (A) and Doppler mode (B).

To improve the imagining surveillance, the American College of Radiology (ACR) released the Ultrasound Liver Imaging Reporting and Data System (US LI-RADS) algorithm in $2017^{[30]}$. According to the LI-RADS algorithm, the size determines the following steps to diagnosis. Lesions measuring less than 1 cm are challenging to be accurately characterised, regardless of the imaging method. Hence, cross-sectional imaging is not required, and short-term follow-up with repeat ultrasonography after 3-4 months is sufficient. If the tumour remains unchanged after two years of surveillance, malignancy is excluded, and the patient returns to the normal screening program. For lesions $\geq 1 \mathrm{~cm}$ in diameter, either quadruple-phase CT or dynamic contrast-enhanced MRI should be performed to establish the diagnosis ${ }^{[11,12]}$.

## Contrast-enhanced ultrasonography

Contrast-enhanced ultrasonography (CEUS) enables physicians to assess the vascular architecture of focal hepatic lesions once detected by depicting the vessels against the background parenchyma. Currently, there are four ultrasound contrast agents (UCAs) approved by the Food and Drug Administration: SonoVue/Lumason (Bracco Suisse SA, Geneva, Switzerland), Definity/Luminity (Lantheus Medical Imaging, Inc., North Billerica, MA, USA), Optison (Perflutren Protein-Type A Microspheres Injectable

Suspension, GE Healthcare, Princeton, NJ) and Sonazoid (GE Healthcare AS, Oslo, Norway) ${ }^{[31]}$. Sonazoid is the only UCA with a hepatic parenchyma-specific Kupffer phase, enabling the physician to obtain images similar to MRI examination ${ }^{[32]}$. In April 2016, the United States Food and Drug Administration (FDA) approved Lumason for intravenous liver applications in children ${ }^{[33]}$.

Based on the arterial enhancement pattern and presence/absence of washout phenomena in the portal venous and delayed phases, the lesion can be characterised by CEUS. As a general rule, the lack of washout during the portal venous and late phase indicates a benign lesion, in which case the arterial enhancement pattern indicates the type of lesion [Figure 5A-C].

The typical contrast behaviour for HCC is arterial hyperenhancement followed by mild late or very late washout (> 60 s$)^{[34,35]}$.

In a recent meta-analysis of 53 studies, Zhang et al. reported that CEUS has a pooled Se of $85 \%$ and a Sp of $91 \%{ }^{[36]}$. For FL $\leq 2 \mathrm{~cm}$, Huang et al. reported a sensitivity of $73.3 \%$ and a specificity of $97.1 \%$, which is comparable to the Se and Sp of $\mathrm{MRI}^{[37]}$.

Contrast enhancement within the thrombus is a pathognomonic sign for tumour thrombosis, while no enhancement indicates benignity. CEUS has been reported to have high sensitivity and specificity ( $90.9 \%$ and $100 \%$, respectively) in diagnosing malignant thrombus ${ }^{[30,31]}$ [Figure 6].

In the NAFLD population, CEUS has a lower performance compared to conventional US due to the selfshadowing of microbubbles and the low mechanical index used during CEUS examination ${ }^{[38]}$.

Putz JF reported that, in patients with limited sound conditions (i.e., obesity and meteorism), the diagnostic accuracy was $92.6 \%$ compared with $98 \%$ in patients with good sound conditions ${ }^{[39]}$. Several strategies may be used to reduce these limitations, such as bringing the FL closer to the transducer (i.e., intercostal positioning of the transducer or supine position) and reducing or increasing the dose of UCA or the mechanical index depending on the FL localisation ${ }^{[40]}$.

EASL guidelines have endorsed CEUS as a second-line tool in patients with main contraindications or inconclusive contrast-enhanced computed tomography $(\mathrm{CT})$ or magnetic resonance imaging (MRI) ${ }^{[9]}$.

## Ultrasound Elastography

Although elastographic techniques, such as point shear wave elastography (pSWE) and 2D-Shear wave elastography (2D-SWE), have been used for staging and monitoring liver fibrosis, several authors have used these techniques to evaluate the FL stiffness. According to the published data, benign FLs are softer than their malignant counterparts and indicate an ascending order of stiffness of FLLs: haemangiomas < FNH < $\mathrm{HCC}<$ metastases $^{[36,4]]}$. Of note, Dong et al. found an overlapping of the rigidity between different lesions, such as between HCC and FNH ${ }^{[42]}$. These overlaps result from the presence of fibrous tissue and the degree of vascularisation in the focal lesion; fibrous tissue tends to increase stiffness, while highly vascularised lesions tend to be softer ${ }^{[43]}$.

The deep location of FL, more than 8 cm from the skin, does not allow the measurement of stiffness ${ }^{[44,45]}$. Obesity seems to limit the successful rate of valid measurements of SWE. A meta-analysis by Hu X found that patients with successful SWE measurements had a lower body mass index than those with unsuccessful measurements ${ }^{[46]}$. Another limitation relates to the susceptibility of motion-related factors that can lead to


Figure 5. Incidentally, hyperechoic lesion with a hypoechoic halo in a 23-year-old woman diagnosed with non-alcoholic liver steatosis. A CEUS with SonoVue was performed. In the early arterial phase, there was a rapid spoke-wheel enhancement of the lesion (arrows) from the centre to the periphery (A). In portal venous (B) and late phase, the lesion remained iso-enhanced compared with adjacent liver parenchyma, indicating that the lesion is benign (C).


Figure 6. Thrombosis of portal vein (main, right and left branch) in a 62-year-old man recently diagnosed with NASH-related cirrhosis. At CEUS examination, with SonoVue, the thrombus presented arterial hyperenhancement (A) with washout in the late phase (B).
an inaccurate value, especially for lesions located in the left lobe. Furthermore, a high liver stiffness (i.e., cirrhosis) increases through compression the stiffness of a FL, making it difficult to differentiate a malignant lesion from a benign lesion ${ }^{[47]}$.

Nevertheless, despite being an imperfect diagnostic tool, the US elastography adds a new dimension to conventional US by providing additional information concerning the FL stiffness. Currently, ultrasound elastography is not recommended for the characterisation of FLs; however, in a few situations, FL stiffness may orientate the diagnosis ${ }^{[48]}$. Therefore, further studies are required to evaluate the accuracy of this method in the characterisation of FLs, especially in NAFLD patients.

Table 1 summarises the indications, advantages and disadvantages of conventional US, CEUS and US elastography

## Artificial Intelligence as a potential future alternative

Artificial intelligence (AI) is a promising tool for radiologic diagnosis in several research studies with potential future applications in clinical practice. In medicine, two approaches have demonstrated promising results: machine learning (ML) and deep learning (DL) models. ML is a branch of AI based on the idea that the system can automatically improve based on its own experience. DL represents a subtype of ML models inspired by the neuroanatomy of the human brain, which uses many layers of artificial neurons called neural networks ${ }^{[49]}$. Convolutional neural networks (CNNs) are a subtype of DL that specialises in processing imaging data.

Despite the positive results, AI is confronted by several issues (i.e., the lack of standardisation of the used algorithms and software, the scarcity of data required to train the system, and the fact that data processing is still incomprehensible to users) that need to be resolved in order to become a reliable diagnostic tool in

Table 1. Indications, advantages and disadvantages of ultrasound and new derived branches

| Method | Indications | Advances | Disadvantages |
| :---: | :---: | :---: | :---: |
| Ultrasonography | HCC surveillance for high-risk patients Guide percutaneous interventions (biopsies, MWA, RFA) | Inexpensive; fast, can be performed bedside; real-time; repeatable; no radiation exposure | Operator, patient and device dependency; deep location (i.e., VII, VIII, IV a) or subcapsular lesions might not be identified; cannot establish the nature of the lesion. |
| CEUS | Lesions' characterisation (i.e., malignant/benign, vascular malformation); <br> guiding the percutaneous interventions (e.g., biopsy, MWA, RFA) | Real-time evaluation; <br> relatively inexpensive; <br> no induced nephrotoxicity and low-risk allergic <br> reactions; <br> repeatable; <br> can depict the vascularity, allowing not only lesions' characterisation but also the necrotic/viable areas or inconspicuous lesions on US <br> Has a higher accuracy in characterising pseudovascular lesions than CT or MRI (i.e., shunts) | Operator, patient and device dependency; cannot characterise deep or subcapsular located lesions; can evaluate only one lesion; thus, for multiple lesions located in different segments, multiple injections are needed Cannot exclude extrahepatic metastasis, and thus cannot be used for staging |
| US elastography | Evaluates liver stiffness; evaluates focal liver lesion's stiffness | Non-invasive method; repeatable; inexpensive | Operator, patient and device dependency; deeply located lesions cannot be evaluated; high sensitivity to motion (i.e., movements induced by heart, non-compliant patients); sampling bias; overlapping stiffness values between malignant and benign lesions |

US: Conventional ultrasound; CEUS: contrast-enhanced ultrasound; CT: computer tomography; MRI: magnetic resonance; MWA: microwave; RFA: radiofrequency ablation.
clinical practice ${ }^{[50]}$.

Table 2 summarises several studies that have evaluated the feasibility of US-based AI in the diagnosis of HCC.

## CONCLUSION

Conventional US is the mainstay in screening HCC high-risk patients. However, despite all the advantages and progressions made in ultrasonography, this method remains operator- and patient-dependent, which represents a real challenge, especially in the NAFLD-related HCC population.

The development of AI could potentially improve the power of US-based methods and, finally, benefit the patient for the early detection of NAFLD-related HCC. In the future, patients at risk of NAFLD-HCC may be screened using a combination of sonography imaging with liquid biopsy.

Table 2. Studies evaluating the feasibility of US-based artificial intelligence in the diagnosis of hepatocellular carcinoma

| Autor, year | Images <br> $(\boldsymbol{n})$ | Method | Al vs, experienced physician <br> (\%) | FLL detection and <br> characterisation | Reference |
| :--- | :--- | :--- | :--- | :--- | :--- |

HCC: Hepatocellular carcinoma; NA: not available; Se: sensitivity, Sp: specificity; ML: machine learning; DL: deep learning; CNN: convolutional neural networks.

## DECLARATIONS

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## Authors' contributions

Literature review and drafted the manuscript: Radu P
Critical review of the manuscript for important intellectual content: Dufour JF
All authors approved of the final version.
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## Conflicts of interest

All authors declare that there are no conflicts of interest.

Ethical approval and consent to participate
Not applicable.

## Consent for publication

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