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- 2 Corrective saccades in acute vestibular neuritis: studying the role of prediction using
- 3 automated passively-induced head impulses

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## 27 ABSTRACT (250 words)

28 When the demands for visual stabilization during head rotations overwhelm the ability of the 29 vestibulo-ocular reflex (VOR) to produce compensatory eye movements, the brain produces 30 corrective saccades that bring gaze towards the fixation target, even without visual cues 31 (covert saccades). What triggers covert saccades and what might be the role of prediction in 32 their generation are unknown. We studied 14 subjects with acute vestibular neuritis. To minimize variability of the stimulus, head impulses were imposed using a motorized torque 33 34 generator with the subject on a bite-bar. Predictable and unpredictable (timing, amplitude, 35 direction) stimuli were compared. Distributions of covert corrective saccade latencies were analyzed with a 'LATER' (linear approach to threshold with ergodic rate) approach. On the 36 37 affected side, VOR gain was higher (0.47±0.28 vs. 0.39±0.22, p<<0.001) with predictable 38 than unpredictable head impulses, and gaze error at the end of the head movement was less 39  $(5.4\pm3.3 \text{ vs } 6.9\pm3.3 \text{ deg p} << 0.001)$ . Analyzing trials with covert saccades, gaze error at 40 saccade end was significantly less with predictable than unpredictable head impulses (4.2 41  $\pm 2.8$  vs 5.5  $\pm 3.2$  deg, p<<0.001). Furthermore, covert corrective saccades occurred earlier with predictable than unpredictable head impulses ( $140\pm37$  vs.  $153\pm37$  ms p<<0.001). Using 42 43 a LATER analysis with reciprobit plots, we were able to divide covert corrective saccades into two classes – early and late – with a break point in the range of 88-98ms. We 44 45 hypothesized two rise-to-threshold decision mechanisms for triggering early and late covert 46 corrective saccades, with the first being most engaged when stimuli are predictable.

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48 Key words: Head impulse, acute vestibular neuritis, saccades, prediction, LATER analysis

#### 49 New & Noteworthy

We successfully used a LATER (linear approach to threshold with ergodic rate) analysis of
the latencies of corrective saccades in patients with acute vestibular neuritis. We found two
types of covert saccades: Early (<90ms) and late (>90ms) covert saccades. Predictability lead
to an increase in VOR gain and a decrease in saccade latency.

# 54 INTRODUCTION

55	The angular vestibulo-ocular reflex (VOR) is mediated by a three neuron arc that stabilizes
56	gaze on a stationary target during head rotations by generating equal and opposite eye
57	rotations (1-4). If the peripheral vestibular system is impaired, or head acceleration or velocity
58	exceeds the capabilities of the vestibular system (5, 6), the VOR cannot generate the correct
59	response to maintain stable gaze. In this case, other mechanisms compensate for the deficient
60	VOR including corrective saccades that tend to bring the image of the target back to the
61	fovea. These saccades are triggered in the direction of the deficient eye movement both when
62	the head is still moving (covert saccades) and after head has stopped (overt saccades) (7-10).
63	The clinical head impulse test (HIT) assesses vestibular function with brisk, passive rotations
64	of the head in the plane of parallel semicircular canal pairs (11). With the bedside HIT
65	clinicians can usually detect overt corrective saccades after the head movement has stopped
66	but covert saccades, made while the head is rapidly rotating, are much harder to discern at the
67	bedside.
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79	passive, if head motion is predictable (15, 22, 23). These findings suggest that corrective
80	saccades are preprogrammed in anticipation of uncompensated head motion.
81	
82	The problems with most of these studies are that with head impulses imposed by hand the
83	ability to infer mechanisms is hindered because of trial-by-trial variability of the stimulus. In
84	previous attempts to standardize head- and body movements using computer controlled
85	rotational body en bloc impulses (crHIT) (18, 24), the stimuli had lower accelerations than
86	conventional head impulses, which did not challenge the capabilities of the VOR to the same
87	degree as higher-acceleration manual head impulses.
88	
89	The main goal of our study was to determine how the brain estimates head velocity when
90	labyrinthine function is deficient or absent, and in turn, how that information is used to
91	generate corrective saccades. Here, we used an automated high acceleration HIT device
92	(aHIT) (25) to analyze corrective saccades in response to standardized passive head impulses
93	in patients with acute vestibular neuritis. Comparing responses to predictable versus
94	unpredictable head impulses, we measured the latencies of the first corrective saccades and
95	the gaze error at their beginning and end. To further focus on mechanisms underlying the
96	generation of non-visually guided corrective saccades (covert saccades) we applied the
97	LATER model (linear approach to threshold with ergodic rate, Carpenter and Williams (26)),
98	which has been used to infer mechanisms for triggering saccades to visual targets.
99	
100	MATERIAL AND METHODS
101	Patients with acute vestibular neuritis

- 102 Patients with acute vestibular neuritis were enrolled as part of a prospective cross-sectional
- study of patients seen in ED (DETECT—Dizziness Evaluation Tool for Emergent Clinical

Triage). We excluded patients younger than 18 years, if symptoms lasted < 24 h or if the 104 105 index ED visit was > 72 h after symptom onset. We also excluded patients with other 106 neurological symptoms or signs, new hearing symptoms, or with previous eye movement or 107 vestibular disorders. All patients with acute vestibular neuritis had caloric irrigations, video 108 head impulse tests (vHIT) and a delayed MRI (3-21d after symptom onset), which served as a gold standard for excluding stroke. Patients with a negative MRI and either a pathological 109 110 HIT or pathological caloric test were diagnosed as acute vestibular neuritis. We also collected 111 information on age and gender.

## 112 Experimental Paradigm

113 Head impulses were performed using an automated device (aHIT<sup>TM</sup>) (25) positioned on a

table in front of the seated subject and consisting of a silicone mouthpiece moving on a

115 curved track. Eye and head movements were recorded using an EyeSeeCam<sup>TM</sup> VOG system

with an integrated full inertial measurement unit (IMU) within the VOG infrared camera at a

117 sampling rate of 220Hz.

118 The patient was seated upright, and the height of the chair was adjusted so that the silicone

119 bite bar was at a comfortable level for the subject. The bite bar was also adjusted with a spirit

120 level to ensure that the axis of rotation was centered about the vertical axis of the subject's

head. During head rotations, the patient was asked to bite down on the bite bar firmly to

ensure transfer of forces from the motor. All head impulses were delivered in the horizontal

123 plane.

124 The aHIT<sup>TM</sup> device was programmed to deliver Gaussian motion profiles with peak angular

velocity of either  $150^{\circ}$ /s or  $250^{\circ}$ /s, both with peak acceleration  $3000^{\circ}$ /s<sup>2</sup>, i.e., the maximum

acceleration deliverable by the device.

127 In a first step a predictable paradigm was performed with a predictable direction, velocity,

amplitude, and timing/cadence between each head impulse. We delivered 10 automated cycles

in the horizontal plane, with each cycle consisting of one impulse to the left and one to the right. The first head impulse always started from the center to lateral position (centrifugal) and the following impulse was from side-to-center (centripetal). Two different types of predictable stimuli were used for each patient: one programmed to reach peak angular velocities of  $150^{\circ}$ /sec with an amplitude of  $10^{\circ}$ , and the other peak angular velocities of  $250^{\circ}$ /sec, with an amplitude of  $20^{\circ}$ . The timing between the head impulses was constant at 1.2 s.

In a second step, an unpredictable paradigm was used, in which the examiner triggeredautomated head impulses, always starting from the center position random in direction (right

138 left), timing (range of 2-5 seconds) and with two pairs of fixed speed and amplitude. We used

139 a random sequence generator for test condition and order.

140

#### 141 Data Analysis

142 Data was processed using custom-made Matlab software that identified head and eye 143 movements on individual trials. A first interactive screening of responses selected only those 144 trials in which there were no artifacts on the eye position trace including contaminating eye 145 blinks, noise due to failed pupil detection/segmentation by the recording software, 146 anticipatory eye movements and slippage of the goggles as indicated by the eyes moving before the initiation of the head movement (27, 28). About 20% of trials were discarded at 147 148 this stage. Corrective saccades were then automatically detected on the high-pass filtered eye 149 velocity trace based on the start (s) and end (e) points when eye velocity rose above or fell 150 below, respectively, 10°/s. Identification of corrective saccades was confirmed by the 151 investigators for each trial. Signal processing was as previously described by Colagiorgio & al 152 (22). The threshold for detecting the onset of head movement was lowered to 5 deg/s given 153 the robotic nature of the stimulator. The gain of the VOR response was calculated as the mean

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of the ratio between horizontal eye velocity and horizontal head velocity computed over the time interval between the times of peak acceleration and peak velocity of the head.

156 We calculated the gaze error defined as the difference between head position and eye position 157 at the beginning of the first corrective saccade, and the total error, for which the saccade must 158 compensate, which was defined as the difference between head position at the end of the saccade and eye position at the beginning of the saccade. In addition, we calculated the gaze 159 error at the end (zero-crossing) of each head impulse. We defined 'covert saccades' as those 160 161 corrective saccades that began before the first zero-crossing of head velocity after the onset of 162 the head impulse. All corrective saccades beginning after the zero-crossing were considered 163 'overt'.

164 The distributions of latencies of covert corrective saccades were interpreted using the LATER model of response time (29), which hypothesizes that the reciprocal of latency in motor 165 responses follows a Gaussian distribution. It considers decision-making processes as a build-166 167 up of activity towards a threshold of confidence, triggering a response, e.g., a saccade, when 168 such a level is reached ( $\tau$ ). The model considers the prior probability of a response-evoking 169 stimulus as the starting point  $S_0$  of such build-up of activity, which will occur with a rate r that 170 is drawn from a Gaussian distribution with mean  $\mu$  and standard deviation  $\sigma$ . We opted for the LATER model because it has been shown to succinctly and quantitatively account for saccade 171 172 reaction time data in a range of saccade behavioral and decision making tasks (e.g. reading, 173 optokinetic responses, anti saccades, prosaccades, etc). Furthermore it does so with few 174 parameters i.e., the mean and variance of the rate of rise of the activity leading to a response 175 (30, 31). We hypothesized that the variability in the latency of corrective saccades in response 176 to head impulses could be interpreted using this model considering two competing processes 177 with build-up rates drawn from two different distributions, one responsible for triggering covert saccades and the other triggering overt saccades. The data is presented on a reciprobit 178

7

179	plot in which the cumulative distribution of saccade latencies is drawn on a probit scale (y-
180	axis) as a function of saccade latency represented on a reciprocal time axis. The reciprobit
181	data was then fit with two straight lines, as for visually driven saccades in [26], using a least
182	mean squares algorithm.
183	Ethics
184	The institutional review board approved this study (KEK#047/14; approval date 04/24/2014).
185	All patients gave written informed consent.
186	
187	RESULTS
188	
189	Stimulus Characteristics
190	We performed 1067 predictable and 1126 unpredictable head impulses on 15 patients with
191	acute vestibular neuritis using the aHIT device. Due to procedural errors, patient #1 had only
192	unpredictable head impulses, while patient #6 had only predictable ones. Their data was
193	included in all population level analyses. After the first screening of eye and head movements
194	we accepted 477 predictable and 606 unpredictable head impulses. Pooling data from all
195	subjects, fast head impulses, programmed at 250 deg/s peak head velocity, achieved a peak
196	head velocity of 245±34 deg/s and lasted 190±10 ms, while slow head impulses, programmed
197	at 150 deg/s achieved 163±23 deg/s and lasted 130±20 ms.
198	The durations of fast and slow impulses were not statistically different between predictable
199	and unpredictable trials. Peak head velocities of slow impulses were not statistically different
200	between predictable and unpredictable trials. Peak head velocities of fast impulses were
201	slightly different with predictable trials being 240 $\pm$ 20 deg/s and unpredictable trials 249 $\pm$ 26
202	deg/s (p<0.01). A more detailed analysis looking at individual subjects highlighted a few
203	patients who had more variability of peak head velocity, possibly due to fluctuating stiffness

of the neck muscles, or some decoupling of the head from the bite bar. The intra-subject

variability of peak head velocity, expressed in terms of its standard deviation in the different

206 paradigms, ranged between 2.5 and 19.4 deg/s.

207

208 *Responses to head impulses* 

- 209 Considering all subjects, the VOR gain in response to head impulses to the pathological side
- was greater with predictable  $0.47\pm0.28$  than unpredictable  $0.39\pm0.22$  stimuli (p<<0.001).

211 There was no statistical difference in VOR gain toward the healthy side comparing the

response to predictable  $(0.87\pm0.11)$  versus unpredictable  $(0.85\pm0.12)$  head impulses.

213 Covert corrective saccades were present in 63.5% of responses to predictable and in 51.5% of

responses to unpredictable head impulses. Figure 1 illustrates two examples of head- and eye

velocity profiles from the fast predictable and unpredictable head impulse stimuli in two

216 representative subjects. With prediction, covert corrective saccades occurred earlier and their

217 amplitudes were higher (Fig. 1).

218

219 *Gaze Error* 

220 Gaze error at the end of the head movement (head velocity crossing zero) was 5.4±3.3 degrees with predictable and  $6.9\pm3.3$  degrees with unpredictable head impulses (p<<0.001) (Fig. 2). 221 222 Including both overt and covert corrective saccades at the end of the first corrective saccade 223 gaze error was  $3.6\pm2.7$  degrees in predictable and  $4.1\pm3.2$  degrees in unpredictable head 224 impulses (p=0.066) (Fig. 3, right hand panel). Considering only covert corrective saccades the 225 gaze error at the end of the first saccade was  $4.2\pm2.8$  degrees with predictable and  $5.5\pm3.2$ 226 degrees with unpredictable head impulses ( $p \le 0.001$ ) (Fig. 3, left hand panel). The gaze error 227 at the beginning of the first corrective saccade was 6.0±4.3 degrees with predictable and 228  $7.4\pm4.3$  with unpredictable head impulses (p<<0.001) (Fig. 4, right hand panel). When 229 considering only covert corrective saccades the gaze error at the beginning of the first

corrective saccade was  $6.7\pm4.5$  with predictable and  $8.7\pm4.2$  with unpredictable head

231 impulses ( $p \le 0.001$ ) (Fig. 4, left hand panel).

232

## 233 Corrective saccades: Latencies and distribution

234 Considering all first corrective saccades, for head impulses toward the affected side the

latency was  $159\pm48$  ms with predictable and  $180\pm52$  ms with unpredictable head impulses

(p << 0.001) (Fig. 5, right hand panel). Considering only covert corrective saccades, for head

impulses toward the affected side the latency was  $140\pm37$  ms in predictable head impulses

and  $153\pm37$  ms in unpredictable ones (p<<0.001) (Fig. 5, left hand panel). For head impulses

toward the healthy side, considering all first corrective saccades, latencies were  $262\pm95$  ms

and  $250\pm89$  ms, for predictable and unpredictable head impulses, respectively, which were

241 not significantly different (p=0.52).

242

## 243 *LATER analysis and model simulation*

244 The reciprobit plot presenting the LATER analysis of latencies of covert corrective saccades 245 toward the pathological side shows two distributions for responses to both predictable and 246 unpredictable head impulses (Fig. 6), with earlier covert saccades represented by the shallower line and later covert saccades by the steeper line. The break point in the fit of 247 248 latencies was at 86 ms for unpredictable impulses and at 97 ms for predictable head impulses. 249 Based on the data shown in Fig. 5, for predictable stimuli the mean saccade latency of early 250 covert saccades was 64±13ms (range 36 and 81 ms) and for late covert saccades 115±18 ms 251 (range 86 and 159ms,). For unpredictable stimuli, the mean saccade latency of early covert 252 saccades was 80±19ms (range 36 and 95 ms) and for late covert saccades 124±17ms (range 253 100 and 195 ms). 254 Based on a model from Noorani and Carpenter (30), which posits two competing saccade

triggering circuits, Figure 7), we simulated the overall distribution of covert saccade latencies

256	during both predictable and unpredictable head impulses. The model has a "MAIN unit" and
257	an "EARLY unit" (See Figure 7). To simulate the response to unpredictable impulses model
258	parameters for the MAIN unit were threshold $\tau=1$ , a mean rate $\mu=9$ and standard deviation
259	$\sigma$ =1.1, which made decisions in an average of $\tau/\mu$ =0.11 seconds. The EARLY unit of the
260	model had a threshold $\tau_E=1.2$ , a mean rate $\mu_E=0$ and standard deviation $\sigma_E=9.2$ . To simulate
261	the responses to predictable head impulses, only one change was necessary; the threshold of
262	the EARLY unit was decreased to $\tau'_{E}$ =0.9 (Fig. 7). The shifting point between the two
263	distributions of early and late covert saccades latencies was fit at 85 ms for unpredictable head
264	impulses and at 96 ms for the predictable ones.

265

#### 266 DISCUSSION

267 In this study we investigated the VOR in patients with an acute vestibular neuritis

268 emphasizing the mechanisms affecting the triggering of corrective saccades and reducing how

269 far the eye is off target (gaze error) during the movement of the head and when the head stops

270 moving (here defined when head velocity crosses zero). Our results support a central role of

271 prediction in the trigger mechanism and reducing gaze error. As previous studies have shown,

272 when head impulses are predictable, a higher proportion of corrective saccades are covert

273 (15). Moreover, both the gaze error at the end of the first corrective saccade and the gaze error

at the end of the head movement were less when head impulses were predictable. This finding

suggests that knowing the direction of head motion is advantageous for the VOR in patients

276 with unilateral loss of function.

## 277 The influence of prediction on the gain of the VOR

278 On the affected side with *predictable* head impulses, the VOR gain was significantly higher

- than with predictable head impulses. On the other hand, there were no significant differences
- in corrective saccade metrics or VOR gain for head impulses to the healthy side. In previous

studies that showed a difference in VOR gain with prediction, the patients either had chronic 281 282 vestibular hypofunction (32) or made active head impulses (20, 33). Previous studies on the 283 interaural translational VOR (tVOR) also showed that expectation had a strong effect on both the gain of the VOR response and on the latency of the first corrective saccade, which were 284 285 respectively higher and lower, respectively, in predictable vs unpredictable trials (34). On the 286 other hand, in a study using passive head impulses in patients after removal of their vestibular 287 schwannomas, the VOR gains were not larger with predictable than with unpredictable 288 impulses (23). Note that in this study, which used manual head impulses and therefore with 289 more stimulus variation compared with motorized head impulses, a different testing paradigm 290 had been used (inward versus outward head impulses). A recent study used the SHIMP 291 (suppression head impulse paradigm) paradigm on healthy subjects, in which the subject 292 fixates upon a target that is rotating with the head, and must make corrective saccades to bring 293 the eyes back to the target after being taken away by the intact VOR (35). Using the SHIMP 294 paradigm with predictable and unpredictable cues, there were higher VOR gains for inward, 295 toward the center, head impulses (35). For the predictable testing paradigm, however, we did 296 not distinguish inward from outward head impulses since the head was moving from center to 297 lateral and vice versa.

298

#### 299 *Corrective saccade latency and prediction*

Corrective saccade latency was significantly greater with unpredictable head impulses, which
accords with previous studies in which latencies of corrective saccades following inward
(presumed predictable) head impulses were lower than those generated during outward (more
unpredictable) head impulses after acute unilateral vestibular nerve deafferentation (15).
A decreased latency of corrective saccades was also reported with active (self-generated) head
impulses (36). Iwasaki et al. studied whole body impulses (rotation *en bloc*) in patients with
unilateral or bilateral vestibular dysfunction and patients showed more overt saccades than

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patients tested with conventional head-on body head impulses, however, the proportion of
covert saccades remained unchanged (18). A tighter clustering of corrective saccades in
response to head impulses, which was also present in some of our patients (Fig. 1) has also
been reported with predictive stimuli (35), active head movements or in the presence of light
(37). We also cannot exclude any quick phase suppression effects during the early phase of a
head impulse (0-60ms), which can be seen, for example, with quick phases of post-rotatory
induced nystagmus (38).

314

### 315 *Saccade accuracy and prediction*

We observed a significantly smaller gaze error with predictable than with unpredictable head impulses for both gaze errors at the end of the head impulse (Fig. 2) and gaze errors at the end of the first covert corrective saccade (Fig 3). These findings suggest that the knowledge of the expected direction and/or speed of head movement during head impulse tests gives the ocular motor system an advantage when using saccades to overcome deficiencies in the VOR.

321

## 322 *Vestibular (covert) saccades versus visually induced saccades*

323 Relatively little is known about covert corrective saccades, triggered by nonvisual stimuli, 324 compared to saccades induced to visual stimuli. Our study shows that with both predictable 325 and unpredictable head impulses there may be a proportion of covert saccades having 326 latencies below 90ms, i.e., corrective saccades may be triggered earlier with vestibular than 327 with visual stimuli (26). Using the LATER analysis model (26), we analyzed the distributions of the reaction times of covert saccades in analogy to the short-latency visually-induced 328 329 saccades with the head still. Saccades in response to visual targets include express saccades 330 (short latencies ~90ms) elicited with a visual gap stimulus, (fixation target is extinguished 331 before the new visual target appears) (39), longer-latency visually induced saccades with the head still, for example to an overlap stimulus (fixation target remains on after the new visual 332

target appears) and predictive, anticipatory saccades which are generated by expectation of 333 334 the appearance of a target (40). Carpenter et al (31) distinguished three types of visually 335 induced saccades with the head still within the short latency region: express saccades, early saccades and late saccades. While express saccades show a bimodal reaction time distribution 336 337 with a LATER analysis (two slopes separated by one flat, horizontal slope (31)), in our study, early, non-visually induced covert saccades form a subpopulation of saccades lying on a 338 339 shallow slope in a reciprobit plot (figure 6A, right panel) that is distinct from the steeper slope 340 characterizing later covert saccades.

341

342 Similarly, our LATER analysis showed two separate distributions of the latencies of covert 343 saccades in both conditions (predictable and unpredictable head impulses), which are not immediately evident in a cursory view of saccade latency histograms. There was a main 344 345 distribution for saccades occurring later than about 90ms (late covert saccades) and an early 346 one for those occurring earlier (<90ms) (early covert saccades, Fig.6). To account for these 347 distinct distributions we propose two rise-to-threshold decision mechanisms for triggering saccades in this time frame. One mechanism triggers most corrective saccades, which 348 349 occurred toward the end of the time window. The other mechanism triggers the earliest saccades (< 90ms after the head movement begins). Terms such as 'covert' or 'overt' 350 351 saccades are derived from clinically performed HITs and describe the ability of the physician 352 to discern saccades. This qualitative terminology, however, might be better supplanted when 353 quantitative eye movement recordings are available. They allow for a quantitative 354 classification of corrective saccades based on timing relative to the parameters of the head 355 movement. Saccades occurring <90ms after the head impulse onset might be called "early 356 covert" saccades.

357

358 Initiation and triggers of early corrective saccades

14

359 We found a significantly smaller gaze error with predictable head impulses at the onset of the 360 first corrective saccades (Fig. 4). We did not find a constant threshold or cluster of gaze errors 361 as a triggering cue for initiation of corrective saccades. Naturally, the lower saccade latencies with predictable head impulses led to smaller gaze errors at saccade onset because the gaze 362 363 position error increases over time during head impulses in patients with a deficient VOR. Thus, we suggest that the covert saccades are not triggered by a fixed threshold based on the 364 365 estimated gaze error, but other factors are also important (prediction, other sensory cues, and 366 inherent variability (noise) in threshold triggering mechanisms).

367

368 What do we learn from the LATER MODEL and reciprobit plots?

369 The LATER model (linear approach to threshold with ergodic rate) was first introduced by

370 Carpenter and Williams (26) in order to study distribution of reaction times of saccades in

response to a visual stimulus (41-44). They described a simple stochastic model to account for

both the random and systematic variation in the saccade latency. When plotted as

373 conventional frequency histogram, the distribution of saccade latencies to the sudden

appearance of a new visual target is skewed (26). Thus, when plotted using a reciprocal scale

for latency, the distribution becomes relatively symmetrical and Gaussian (Fig. 6, left panel).

376 By plotting our data on a probit scale (y-axis, in effect an inverse error function

transformation) and the covert saccade latency on a reciprocal scale (x-axis), we obtained a

reciprobit plot which we fitted using two straight lines (Figure 6A, right panel) similar to

those proposed by Carpenter & al. (1995). Thus, the LATER model may be also suitable for

analysis of early, nonvisual "covert" corrective saccades generated when the VOR is

381 deficient.

382 In our study, the cumulative probability of early covert saccades in the reciprobit plots was

higher with predictable head impulses. Thus this approach provides a way to quantify the

384 effects of various cues, including predictability, that have been previously shown to improve

VOR performance with not only a reduction and clustering of the corrective saccades
latencies but also a decrease in gaze error at the end of the first corrective saccades. In the
case of predictability, important factors might include prior knowledge and expectation based
on timing, direction, movement profile (velocity, size of excursion), and eventually resulting
in internally generated movement commands.

390 Interestingly, the distribution of latencies of covert saccades' on the reciprobit plot showed a 391 similar pattern to the short-latency saccades that occur with visual targets (26). Thus, we 392 hypothesize that nonvisual corrective saccades during head impulses may be initiated by 393 competing stochastic decision mechanisms for signal processing in the brain based on the 394 different available cues, and that the winning mechanism, i.e., the one reaching the threshold 395 sooner, determines when the brain should initiate a corrective saccade. These stochastic 396 mechanisms are important, since sensory input signals are noisy (biological noise) and the 397 brain needs to make an inference about the actual performed head movement and the needed 398 eye correction. We simulated our results with a two decision mechanisms LATER model 399 suggesting that with prediction the threshold for generating early covert saccades is reduced; a 400 change that reflects greater confidence in the predictive mechanism that triggers the earliest 401 corrections. In a Bayesian sense, the threshold was considered a prior and was adjusted 402 accordingly based on stimulus predictability. 403 What might be the anatomical substrate for these circuits that trigger non-visual early and late 404 covert saccades? In analogy with visually guided saccades, it may be that direct subcortical, 405 mechanisms, perhaps mediated by short-latency visual drives to the superior colliculus 406 account for early visually-guided or even 'express' saccades. The cerebellum, too, has been

- 407 implicated in the generation of express saccades since asymmetrical lesions of the dorsal
- 408 vermis abolish express saccades in one direction (45). Saccade (quick phase) related activity
- 409 for vestibular nystagmus has also been recorded in so-called burster driver neurons in the

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410 medulla (46). How these various circuits relate to generating covert saccades remains to be411 discovered.

412

### 413 *Limitations of the study*

414 We used an automated head impulse device in the attempt to provide a more reproducible 415 vestibular stimulus and so minimize some of the variability of stimulus parameters that might 416 confound the interpretation of corrective saccade timing and amplitude in patients with a 417 deficient VOR. A standardized HIT technique is important when analyzing corrective 418 saccades since gaze error and saccade latency are functions of head velocity and acceleration. 419 Accordingly, variability of the stimulus adds to inherent variability (noise) of the VOR 420 response, which could make statistical inferences more difficult, especially when the number 421 of trials is limited (10). Furthermore, nonlinearities in the ability of an impaired labyrinth to 422 transduce head velocity could make statistical inferences more difficult with a more variable 423 stimulus. Even by using the automated head impulse test, we could not eliminate all 424 variability of head movements because of various factors including neck muscle tension and 425 imperfect coupling of the head to the bite bar. Our results also may not generalize to all 426 patients with loss of vestibular function. We did not study patients with bilateral vestibular 427 loss nor patients with chronic vestibular hypofunction. And there was certainly variability in 428 the degree of vestibular loss when our patients were tested, and the time after onset of illness to time of testing was not the same for all patients allowing recovery and adaptation to take 429 430 place to different degrees in different patients. Examining larger numbers of patients with 431 more trials might allow a better way to test our model. In addition, we did not use a 432 paradigm, such as *en bloc* rotations, to analyze the influence of neck proprioceptive cues on 433 the VOR response. Other factors that should be considered in future studies including 434 increasing the randomness of the stimulus (more than two velocities, more than two 435 amplitudes, different timings, etc).

17

#### 436 CONCLUSIONS

437 In patients with acute vestibular neuritis, we used an automated system to impose

- 438 standardized passive head impulses and showed that predictability decreases the latency of
- 439 corrective saccades, and increases VOR gain. With predictable head impulses the gaze
- 440 position error after the first corrective saccade, and at the end of the head impulse, is reduced
- 441 improving the function of the VOR. Using a 'LATER' analysis of distributions of latencies of
- 442 corrective saccades we were able to see more clearly the patterns shown by covert saccades.
- 443 We found two subtypes of covert saccades: early (<90ms) and late (>90ms). We propose two
- rise-to-threshold stochastic decision mechanisms for triggering early and late covert
- 445 corrective saccades before new visual information becomes available in patients with
- vestibular hypofunction. Predictability primarily impacts the early mechanism, producing
- 447 more early covert corrective saccades.
- 448 The challenge for further studies is to discover the circuits that generate covert corrective
- saccades and the mechanisms by which they are influenced by prediction.

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#### 455 Figure legends

- 456 Fig. 1. Example of recordings in two representative patients (A and B) using the automated
- 457 HIT device showing fast head impulses and the corresponding eye movements (inverted for
- 458 comparison). Panel A shows responses to predictable head impulses with covert saccades
- 459 occurring earlier compared to unpredictable head impulses (Panel B). Panel C shows more
- 460 covert corrective saccades cluster more with predictable than unpredictable head impulses
- 461 (Panel D). Note the lower VOR gain with unpredictable head impulses for both patients.

463 Fig. 2 Box plot of Gaze Error when *the head stops* considering only *covert saccades* after

464 predictable (Pred) vs. unpredictable (Unpred) head impulses in patients with acute vestibular

465 neuritis. Left: The gaze error in head impulses to the affected side is significantly higher when

- these are unpredictable. Right: The gaze error in head impulses to the healthy side is also
- 467 significantly higher when these are unpredictable.
- 468

Fig. 3, left: Box plot of Gaze Error at *the end of covert corrective* saccades after predictable

470 (Pred) vs. unpredictable (Unpred) head impulses in patients with acute vestibular neuritis. The

471 gaze error in head impulses to the affected side is significantly higher when head impulses are

472 unpredictable. Right: Box plot of gaze error at *the end of the first saccade*, considering all

trials with a corrective saccade after predictable (Pred) vs. unpredictable (Unpred) automated

474 head impulses. The gaze error between predictable and unpredictable head impulses to the

- 475 affected side is not significantly different.
- 476

477 Fig. 4. Left: Box-plot of Gaze Error at the onset of covert saccades in predictable (Pred) vs.

unpredictable (Unpred) head impulses. The gaze error at the end of the saccade was

significantly higher in unpredictable head impulses to the affected side. Right: Box plot of

480 gaze error at the *onset of the first saccade* in predictable (Predict) vs. unpredictable

481 (Unpredict) automated head impulses. The analysis shows that the gaze error between

482 predictable and unpredictable head impulses to the affected side is significantly different.

483 Fig. 5. Left: Box-plot of all *first covert corrective* saccade latencies in predictable (Pred) vs.

484 unpredictable (Unpred) head impulses. Saccade latency was significantly higher in

485 unpredictable head impulses to the affected side. Right: Box plot of corrective saccade latency

486 considering *the first corrective saccade* in predictable (Predict) vs. unpredictable (Unpredict)

- automated head impulses. The analysis shows that the gaze error between predictable and
  unpredictable head impulses to the affected side is significantly different.
- 489 Fig. 6A: The LATER based analysis of covert corrective saccades in patients with vestibular 490 neuritis after predictable and unpredictable head impulse tests: Left, frequency histogram (x-491 axis: Latency; y-axis: Frequency of saccades); right, reciprobit plot: note that the cumulative 492 probability of early saccades in the reciprobit plots was higher with predictable head 493 impulses. Fig. 6B: Simulation of a two decision mechanisms LATER model in the 494 unpredictable (blue) and predictable (red) conditions. Left panel: distribution of saccade 495 latencies predicted by the model in the two conditions. Right panel: reciprobit plot of simulated latency data and their fit. Parameters for unpredictable head impulses: Main unit 496 with  $\tau=1$ ,  $\mu=9$ ,  $\sigma=1.1$  and Early unit  $\tau_{\rm E}=1.2$ ,  $\mu_{\rm E}=0$ ,  $\sigma_{\rm E}=9.2$ . Parameters for predictable head 497 impulses: Main unit with  $\tau=1$ ,  $\mu=9$ ,  $\sigma=1.1$  and Early unit  $\tau_{E}=0.9$ ,  $\mu_{E}=0$ ,  $\sigma_{E}=9.2$ . 498
- 499
- 500

501 Fig. 7. Scheme of a two competing saccade triggering mechanisms model: a "Main unit" with parameters  $\mu$ ,  $\sigma$  and  $\tau$  operates in parallel with a 'maverick' Early unit, whose parameters are 502  $\mu_E = 0$ ,  $\sigma_E$ . and  $\tau_E$ . Whichever unit reaches threshold first triggers the response. In both 503 mechanisms the decision signal (blue) starts from an initial level  $S_0=0$ . 504 To simulate the response to unpredictable impulses model parameters for the Main unit were 505 506 threshold  $\tau=1$ , a mean rate  $\mu=9$  and standard deviation  $\sigma=1.1$ , which made decisions in an average of  $\tau/\mu=0.11$  seconds. The Early unit of the model had a threshold  $\tau_{E}=1.2$ , a mean rate 507 508  $\mu=0$  and standard deviation  $\sigma_E=9.2$ . To simulate the responses to predictable head impulses, only one change was necessary; the threshold of the Early unit was decreased to  $\tau'_{E}=0.9$ . 509

### 510 **References**

Minor LB, Lasker DM, Backous DD, Hullar TE. Horizontal vestibuloocular reflex evoked by
 high-acceleration rotations in the squirrel monkey. I. Normal responses. Journal of neurophysiology.
 1999;82(3):1254-70.

Aw ST, Haslwanter T, Halmagyi GM, Curthoys IS, Yavor RA, Todd MJ. Three-dimensional
 vector analysis of the human vestibuloocular reflex in response to high-acceleration head rotations. I.
 Responses in normal subjects. Journal of neurophysiology. 1996;76(6):4009-20.

Roy FD, Tomlinson RD. Characterization of the vestibulo-ocular reflex evoked by high-velocity
 movements. The Laryngoscope. 2004;114(7):1190-3.

Tabak S, Collewijn H, Boumans LJ, van der Steen J. Gain and delay of human vestibulo-ocular
 reflexes to oscillation and steps of the head by a reactive torque helmet. I. Normal subjects. Acta oto laryngologica. 1997;117(6):785-95.

5. Peng GC, Zee DS, Minor LB. Phase-plane analysis of gaze stabilization to high acceleration
 head thrusts: a continuum across normal subjects and patients with loss of vestibular function.
 Journal of neurophysiology. 2004;91(4):1763-81.

525 6. Halmagyi GM, Curthoys IS, Cremer PD, Henderson CJ, Todd MJ, Staples MJ, et al. The human
526 horizontal vestibulo-ocular reflex in response to high-acceleration stimulation before and after
527 unilateral vestibular neurectomy. Experimental brain research. 1990;81(3):479-90.

528 7. Bloomberg J, Melvill Jones G, Segal B. Adaptive plasticity in the gaze stabilizing synergy of 529 slow and saccadic eye movements. Experimental brain research. 1991;84(1):35-46.

Schubert MC, Hall CD, Das V, Tusa RJ, Herdman SJ. Oculomotor strategies and their effect on
 reducing gaze position error. Otology & neurotology : official publication of the American Otological
 Society, American Neurotology Society [and] European Academy of Otology and Neurotology.
 2010;31(2):228-31.

534 9. Kasai T, Zee DS. Eye-head coordination in labyrinthine-defective human beings. Brain 535 research. 1978;144(1):123-41.

536 10. Weber KP, Aw ST, Todd MJ, McGarvie LA, Curthoys IS, Halmagyi GM. Head impulse test in
537 unilateral vestibular loss: vestibulo-ocular reflex and catch-up saccades. Neurology. 2008;70(6):454538 63.

Halmagyi GM, Curthoys IS. A clinical sign of canal paresis. Archives of neurology.
1988;45(7):737-9.

Mantokoudis G, Tehrani AS, Wozniak A, Eibenberger K, Kattah JC, Guede CI, et al. VOR gain
 by head impulse video-oculography differentiates acute vestibular neuritis from stroke. Otology &
 neurotology : official publication of the American Otological Society, American Neurotology Society
 [and] European Academy of Otology and Neurotology. 2015;36(3):457-65.

545 13. Zamaro E, Saber Tehrani AS, Kattah JC, Eibenberger K, Guede CI, Armando L, et al. VOR gain
546 calculation methods in video head impulse recordings. Journal of vestibular research : equilibrium &
547 orientation. 2020;30(4):225-34.

548 14. Sjögren J, Fransson PA, Karlberg M, Magnusson M, Tjernström F. Functional Head Impulse
549 Testing Might Be Useful for Assessing Vestibular Compensation After Unilateral Vestibular Loss.
550 Frontiers in neurology. 2018;9:979.

Mantokoudis G, Agrawal Y, Newman-Toker DE, Xie L, Saber Tehrani AS, Wong A, et al.
Compensatory saccades benefit from prediction during head impulse testing in early recovery from
vestibular deafferentation. European archives of oto-rhino-laryngology : official journal of the
European Federation of Oto-Rhino-Laryngological Societies (EUFOS) : affiliated with the German
Society for Oto-Rhino-Laryngology - Head and Neck Surgery. 2016;273(6):1379-85.

55616.Collewijn H, Smeets JB. Early components of the human vestibulo-ocular response to head557rotation: latency and gain. Journal of neurophysiology. 2000;84(1):376-89.

558 17. Macdougall HG, Curthoys IS. Plasticity during Vestibular Compensation: The Role of Saccades.
 559 Frontiers in neurology. 2012;3:21.

18. Iwasaki S, Kamogashira T, Fujimoto C, Kabaya K, Kinoshita M, Yamasoba T. The Role of Neck

Input in Producing Corrective Saccades in the Head Impulse Test. Frontiers in neurology.2022;13:881411.

563 19. Schubert MC, Zee DS. Saccade and vestibular ocular motor adaptation. Restorative neurology 564 and neuroscience. 2010;28(1):9-18. 565 20. Black RA, Halmagyi GM, Thurtell MJ, Todd MJ, Curthoys IS. The active head-impulse test in 566 unilateral peripheral vestibulopathy. Archives of neurology. 2005;62(2):290-3. 567 21. Peng GC, Minor LB, Zee DS. Gaze position corrective eye movements in normal subjects and 568 in patients with vestibular deficits. Annals of the New York Academy of Sciences. 2005;1039:337-48. 569 Colagiorgio P, Versino M, Colnaghi S, Quaglieri S, Manfrin M, Zamaro E, et al. New insights 22. 570 into vestibular-saccade interaction based on covert corrective saccades in patients with unilateral 571 vestibular deficits. Journal of neurophysiology. 2017;117(6):2324-38. 572 23. Schubert MC, Mantokoudis G, Xie L, Agrawal Y. Acute VOR gain differences for outward vs. 573 inward head impulses. Journal of vestibular research : equilibrium & orientation. 2014;24(5-6):397-574 402. 575 24. Furman JM, Shirey I, Roxberg J, Kiderman A. The horizontal computerized rotational impulse 576 test. Journal of vestibular research : equilibrium & orientation. 2016;26(5-6):447-57. 577 25. Tan GX, Schoo DP, Della Santina CC, Rahman MA, Valentin Contreras NS, Sun CH, et al. 578 Automated head motion system improves reliability and lessens operator dependence for head 579 impulse testing of vestibular reflexes. IEEE International Symposium on Medical Measurements and 580 Applications : proceedings IEEE International Symposium on Medical Measurements and 581 Applications. 2017;2017:94-9. 582 26. Carpenter RH, Williams ML. Neural computation of log likelihood in control of saccadic eye 583 movements. Nature. 1995;377(6544):59-62. 584 27. Versino M, Colagiorgio P, Sacco S, Colnaghi S, Ramat S. Artifact avoidance for head impulse 585 testing. Clin Neurophysiol. 2014;125(5):1071-3. 586 Mantokoudis G, Saber Tehrani AS, Kattah JC, Eibenberger K, Guede CI, Zee DS, et al. 28. Quantifying the vestibulo-ocular reflex with video-oculography: nature and frequency of artifacts. 587 588 Audiology & neuro-otology. 2015;20(1):39-50. 589 Carpenter RHS. Oculomotor Procrastination. In: Fisher DF, Monty RA, Laboratory USAHE, 29. 590 editors. Eve Movements: Cognition and Visual Perception. Hillsdale, New Jersey: Lawrence Erlbaum 591 Associates, Inc.; 1981. 592 30. Noorani I, Carpenter RH. The LATER model of reaction time and decision. Neuroscience and 593 biobehavioral reviews. 2016;64:229-51. 594 Carpenter RHS. Analysing the Detail of Saccadic Reaction Time Distributions. Biocybernetics 31. 595 and Biomedical Engineering. 2012;32(2):49-63. 596 Lee SH, Newman-Toker DE, Zee DS, Schubert MC. Compensatory saccade differences 32. 597 between outward versus inward head impulses in chronic unilateral vestibular hypofunction. J Clin 598 Neurosci. 2014;21(10):1744-9. 599 33. Della Santina CC, Cremer PD, Carey JP, Minor LB. Comparison of head thrust test with head 600 autorotation test reveals that the vestibulo-ocular reflex is enhanced during voluntary head 601 movements. Arch Otolaryngol Head Neck Surg. 2002;128(9):1044-54. 602 34. Ramat S, Straumann D, Zee DS. Interaural translational VOR: suppression, enhancement, and 603 cognitive control. Journal of neurophysiology. 2005;94(4):2391-402. 604 35. Starkov D, Vermorken B, Van Dooren TS, Van Stiphout L, Janssen M, Pleshkov M, et al. The 605 Effect of Different Head Movement Paradigms on Vestibulo-Ocular Reflex Gain and Saccadic Eye 606 Responses in the Suppression Head Impulse Test in Healthy Adult Volunteers. Frontiers in neurology. 607 2021;12:729081. 608 36. Sprenger A, Zils E, Stritzke G, Krüger A, Rambold H, Helmchen C. Do predictive mechanisms 609 improve the angular vestibulo-ocular reflex in vestibular neuritis? Audiology & neuro-otology. 610 2006;11(1):53-8. 611 37. Pogson JM, Taylor RL, McGarvie LA, Bradshaw AP, D'Souza M, Flanagan S, et al. Head impulse 612 compensatory saccades: Visual dependence is most evident in bilateral vestibular loss. PloS one. 613 2020;15(1):e0227406.

- Mantokoudis G, Tehrani AS, Xie L, Eibenberger K, Eibenberger B, Roberts D, et al. The video
  head impulse test during post-rotatory nystagmus: physiology and clinical implications. Experimental
  brain research. 2016;234(1):277-86.
- 617 39. Fischer B, Ramsperger E. Human express saccades: extremely short reaction times of goal 618 directed eye movements. Experimental brain research. 1984;57(1):191-5.
- 40. Leigh R, Zee D. The neurology of eye movements. 5th ed. Oxford: Oxford University Press;2015.
- 621 41. Schall JD. Experimental psychology. Race to explain procrastination. Nature.
- 622 1995;377(6544):14-5.
- 42. Posner MI. Timing the brain: mental chronometry as a tool in neuroscience. PLoS biology.2005;3(2):e51.
- 43. Meyer DE, Osman AM, Irwin DE, Yantis S. Modern mental chronometry. Biological
  psychology. 1988;26(1-3):3-67.
- 627 44. Renault B, Ragot R, Lesevre N, Remond A. Onset and offset of brain events as indices of 628 mental chronometry. Science (New York, NY). 1982;215(4538):1413-5.
- 45. Takagi M, Zee DS, Tamargo RJ. Effects of lesions of the oculomotor vermis on eye movements in primate: saccades. Journal of neurophysiology. 1998;80(4):1911-31.
- 46. Hikosaka O, Igusa Y, Nakao S, Shimazu H. Direct inhibitory synaptic linkage of pontomedullary
- reticular burst neurons with abducens motoneurons in the cat. Experimental brain research.
- 633 1978;33(3-4):337-52.

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LATER analysis of covert saccades during predictable and unpredictable head impulses identifies two distributions for covert saccades in acute vestibular neuritis patients, produced by two competing decision mechanisms, which we called early and late covert saccades



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